

# Presentation 2

## Concept Generation and Evaluation

Calcified Vessel Model Team

ME 476C-002

10/9/2024

# Project Description

## Client:

W.L. Gore & Associates, Inc.  
Medical Division



Figure 1 – Gore Logo [1]

## Project Scope:

The scope of this project is to design, build, and test a replicable (12 count) model of calcified lesions in the Peripheral Arterial System for deployment of peripheral vascular interventional devices under simulated use conditions, using non-biologic materials.

## Significance of the Project:

Vascular intervention devices are crucial for treating peripheral arterial disease(s) by restoring blood flow, reducing symptoms, and preventing severe complications through intervention care.

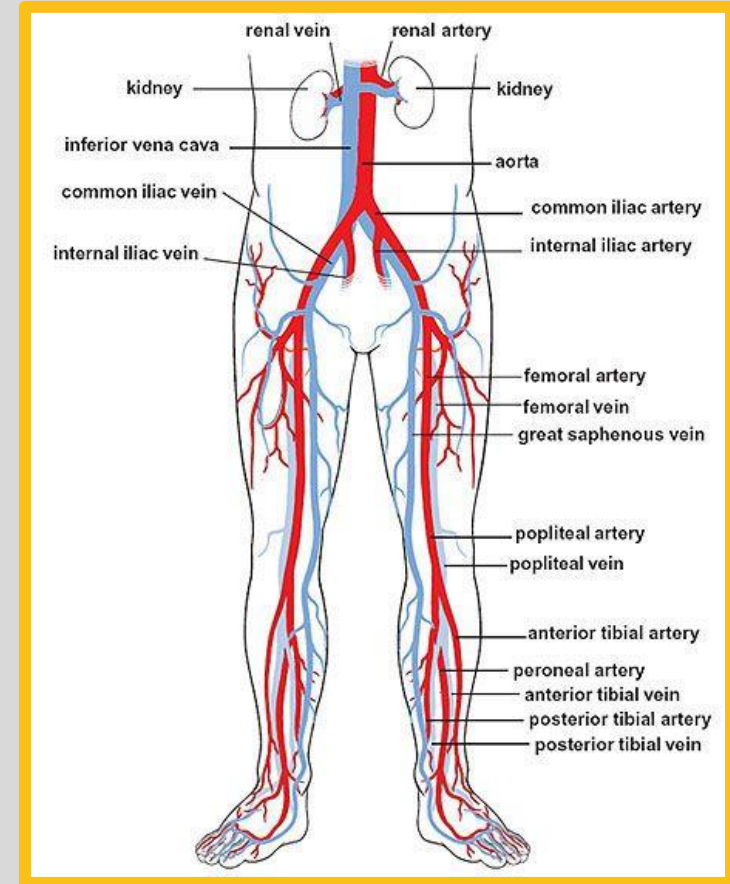
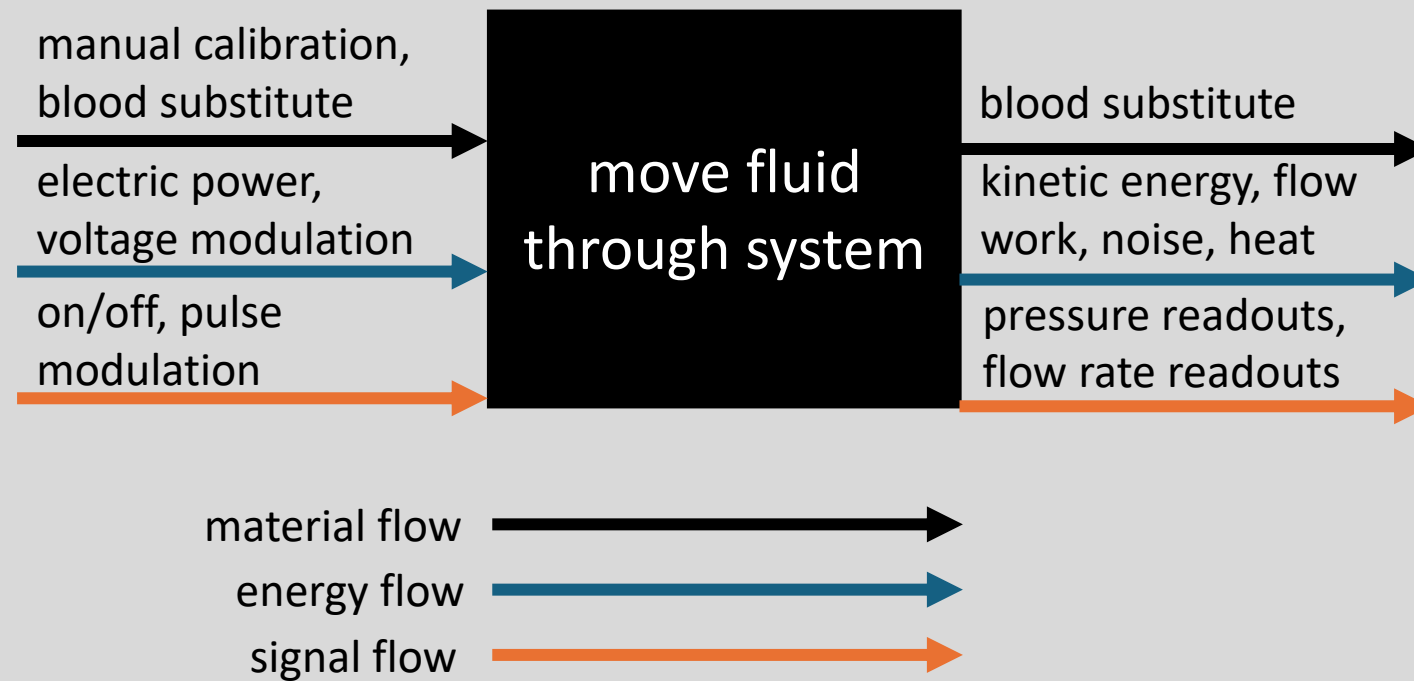


Figure 2 – Peripheral Artery System [1]

# Black Box Model



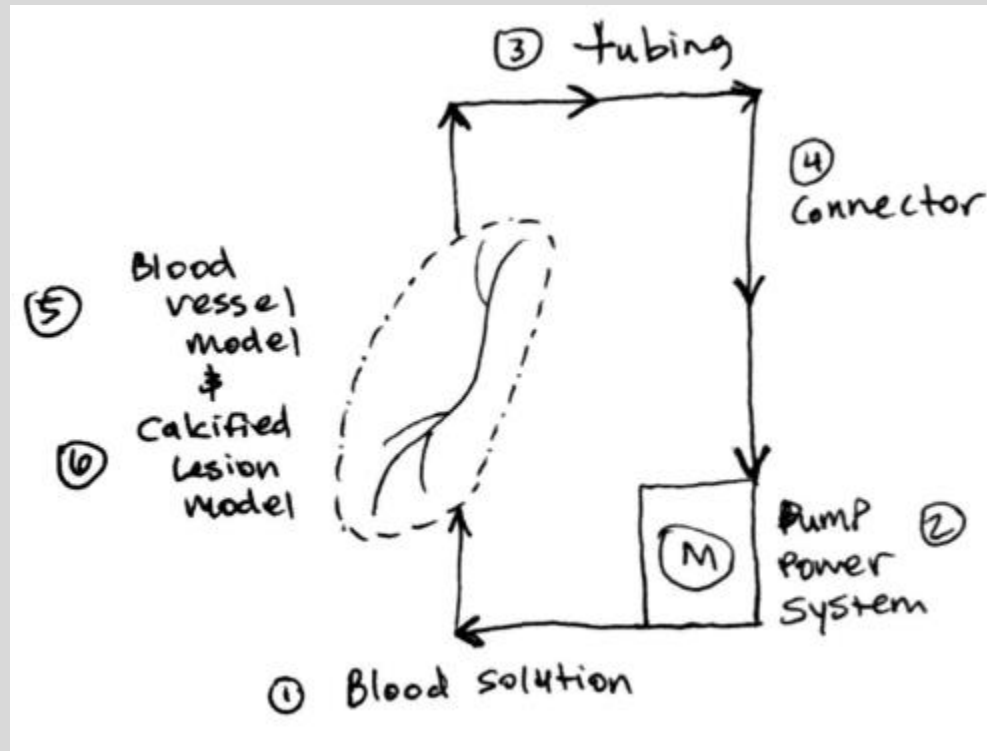
# Physical Decomposition

## System:

Calcified Lesion Vessel  
Simulation Model

## Components:

1. Blood Substitute  
*simulates blood*
2. Power/Pump System  
*produces flow*
3. Tubing  
*directs flow*
4. Connectors  
*connects system*
5. Blood Vessel Model  
*simulates femoral artery*
6. Calcified Lesion Model  
*simulates calcification*



## Hierarchy:

- Power/Pump System
  - >Arduino Kit
    - >>Circuitry
  - >Motor
  - >Pulsatile pump
  - >Tubing
  - >Connector
  - >Reservoir
- Calcified Lesion Vessel Model
  - >Blood Vessel Model
    - >>Femoral artery
  - >Calcified Lesion Model

# Morphological Matrix

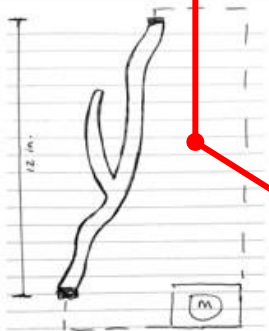
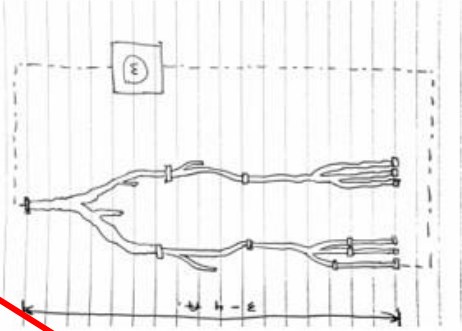
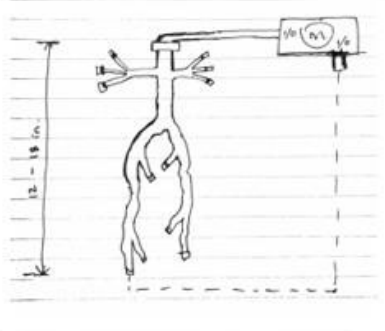






Subsystem	Concept 1	Concept 2	Concept 3
Top Level design			
Lesion Material			
Lesion Adhesion			

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# Morphological Matrix

Final Design

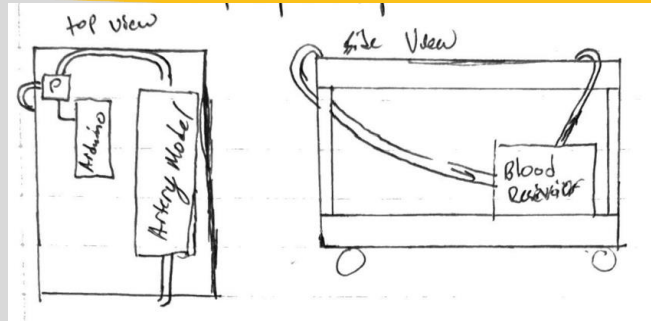
Prototype Only

Subsystem	Concept 1	Concept 2	Concept 3
Vessel Structure			
Vessel Material			
Blood Solution			

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# Concept Generation: Top level Design

## Concepts

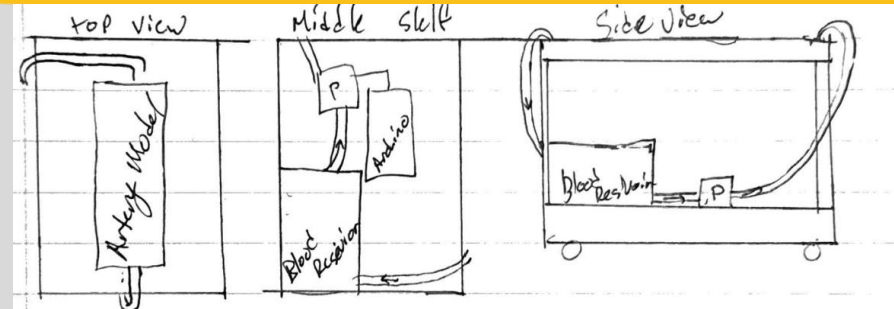


### Computing and pump on top

+ easy access to the computing and pump systems

+ pump at same level as model

- If failure occurs near pump fluid could get into electronics

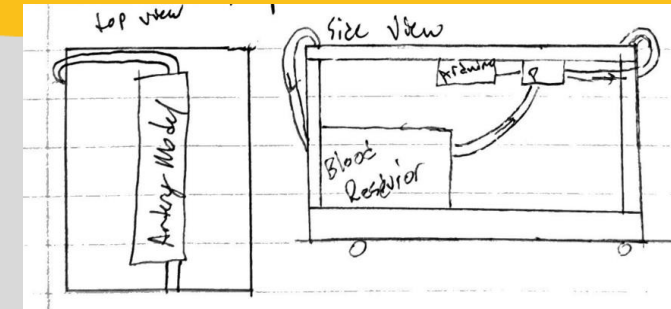


### Computing and pump on bottom

+ only the artery model is showing

- If failure occurs at tank or pump fluid can get on electronics

- Pump might not create enough work to get water to the model



### Computing and pump undermounted

+ only artery model is showing

+ electronics are out of the danger zone if failure occurs

- Accessing the electronics and pump system is more difficult

# Concept Generation/Evaluation: Pump

## Concepts



**3D printed Peristaltic pump**



**Peristaltic Pump**

## Advantages/ Disadvantages

+ allows for full customization of pump power and flow rate

- Will take several hours of development to create a pump that will meet engineering requirements

+ easy to procure, and meets the flow rate requirement

- might need a higher power output to overcome friction loss in pipes

+ perfect for proof of concept in prototyping

## Our decision:

The 3D printable pump would take several modifications to achieve the desired flow rate, therefore a pump that can achieve the flow rate will be purchased for prototyping. If after testing occurs this pump needs to be changed to better fit engineering requirements we can do so.



# Concept Generation/Evaluation: Computing

## Concepts



**Arduino**

+ allows for circuits to be created easily

## Advantages/ Disadvantages

+easily accessible through the school to be able to prototype

-manufacturing of a way to hold all parts is needed



**Raspberry pi**

+ allows for circuits to be created easily

- Creating the code is more difficult

-manufacturing of a way to hold all parts is needed

## Our decision:

Since both will meet the customer needs we will use the easier of the 2 concepts We will use the Arduino since supplies and learning material are readily available.

# Concept Generation: Calcified Lesions

## Material

### High-Hardness 3D Printer Filament [1]



## Advantages/ Disadvantages

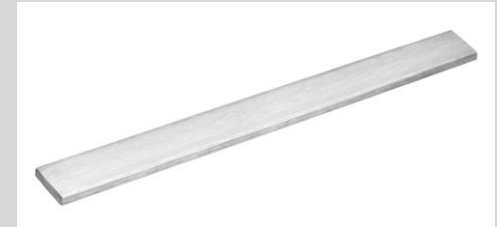
- + Accurate and consistent hardness
- + High resolution
- + Complete control of manufacturing process
- Relatively expensive

### Fired Ceramic [2]



- + Most accurate material properties
- + Easy to manufacture
- + Relatively inexpensive
- Inconsistent hardness
- Low resolution

### Machined Steel [3]

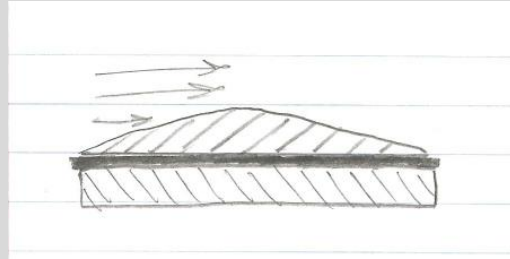


- + Consistent hardness
- + High resolution
- Complex manufacturing process
- Relatively low hardness

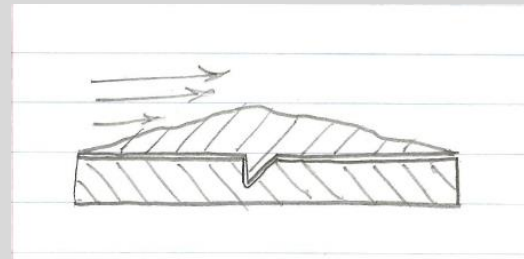
# Concept Generation: Calcified Lesions

## Adhesion Method

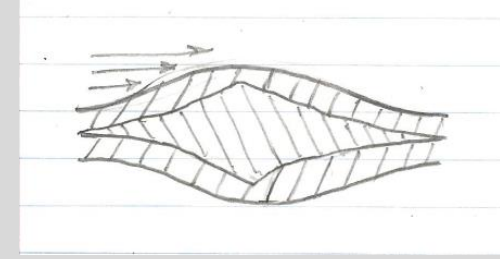
### Adhesive Paste



### Interlocking Mechanism



### Embedded



## Advantages/ Disadvantages

- + Complete control over adhesion strength
- + No protruding geometries
- + Accurate to real-world use conditions
- + No additional manufacturing complexity
- Additional assembly complexity

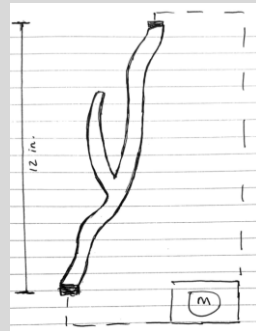
- + Complete control over adhesion strength
- + No additional manufacturing/assembly complexity
- Unidirectional adhesion strength
- Protruding geometries

- + No protruding geometries
- + No additional manufacturing complexity
- Additional assembly complexity
- Adhesion strength determined by vessel wall strength
- Inaccurate to real-world use conditions

# Concept Generation: Blood Vessel Structure

## Vessel Design Structure

### Femoral Artery (R)

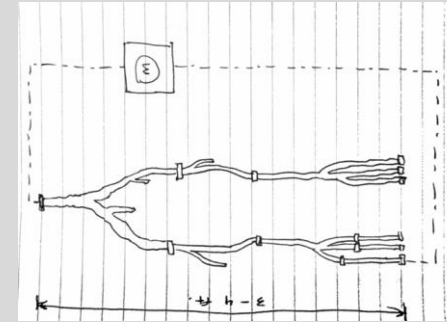


(+/-) Only the right femoral artery in the system

(+) A common vessel site for the occurrence of calcification

(+) With a reduced fluid volume to manage, the system requires less power

### Lower Extremity

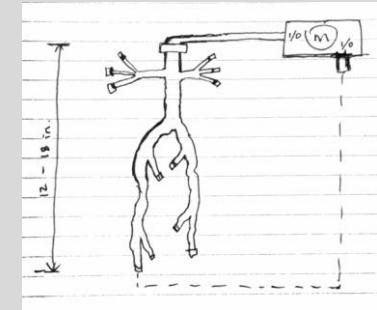


(+) Explore the lower extremity arterial system

(+) Interconnection points for removing and adding vessels

(-) More fluid volume can lead to complications in pump power system

### Femoral Artery



(+) Less fluid volume

(+) Less power required to pump

(+) L/R femoral artery

(+/-) Only the femoral artery in the system

## Advantages/ Disadvantages

# Concept Generation: Blood Vessel Structure

## Material

### Vinyl Tubing (PVC)



- (-) Dimensions are general and are limited in thickness size to 3.2mm
- (-) Only sold in 50 ft rolls
- (+) Clear and transparent
- (-) Adhesion compatibility unknown

### 3D Printing Filament



- (+) Design intentions can be met more accurately
- (+) Hardness: Shore D 76
- (-) Will require a 3D printer or 3D printer services
- (+) Good adhesion compatibility

### Silicone Tubing



- (+) exceptional pump life for peristaltic pumps
- (+) Hardness: Shore A 50; soft material but durable
- (+) sold in various sizes and reasonably priced
- (-) Not exactly transparent

## Advantages/ Disadvantages

# Concept Generation: Blood Solution

## Material

### Glycerin



- +Transparent
- +Non-biological materials
- +No mixing of creating ourselves
- More expensive to buy
- +/- Has safety procedure for use

### Simulated Blood



- +Very similar to blood viscosity and flow
- Not transparent
- +Cheaper option to purchase
- Has no safety procedures
- Limited spec sheet

### Corn Syrup, Water and Flour Mixture



- +Can change the viscosity and flow characteristics
- May contain biological materials
- +Cheapest option
- +No safety procedure for testing needed
- Must be mixed ourselves leaving room for inconsistencies
- May harden if left too long

## Advantages/ Disadvantages

# Concept Generation: Blood Solution

## Material

### Doppler Ultrasound Gel



- +Readily available
- +Cheap to purchase
- Gel does not have fluid properties
- Non-transparent
- Higher viscosity than needed

### Red Blood Cell Surrogates



- +Very realistic for model
- Biological materials
- Not realistic for attaining
- Typically, from healthy patients not sick ones

### PEG 200 Polyethylene Mixture



- +Available for purchase
- +Closely relates to blood properties
- More expensive than other options
- Not available in large quantities that are required
- Long list of procedure for use and safety requirements

## Advantages/ Disadvantages

# Engineering Calculation: Pump Placement

Pump power =  $\dot{W} = \rho Q g H_p$ , [22] Where  $H_p = \left( \frac{p}{\rho g} + \frac{V}{2g} + z \right)_{discharge} - \left( \frac{p}{\rho g} + \frac{V}{2g} + z \right)_{suction}$

then

$$\dot{W} = \rho Q g \left[ \left( \frac{p}{\rho g} + \frac{V}{2g} + z \right)_{discharge} - \left( \frac{p}{\rho g} + \frac{V}{2g} + z \right)_{suction} \right]$$

When assumption is applied

$$\dot{W} = \rho Q g \left( \frac{p}{\rho g} + \Delta z \right)$$

So the head on the pump is dictated by the pressure and the height between pump and the vessel model

We can reduce the total head and therefore the power required by the pump by putting the pump at the same level as the model

Variables:

$$\rho = 1060 \frac{kg}{m^3}$$

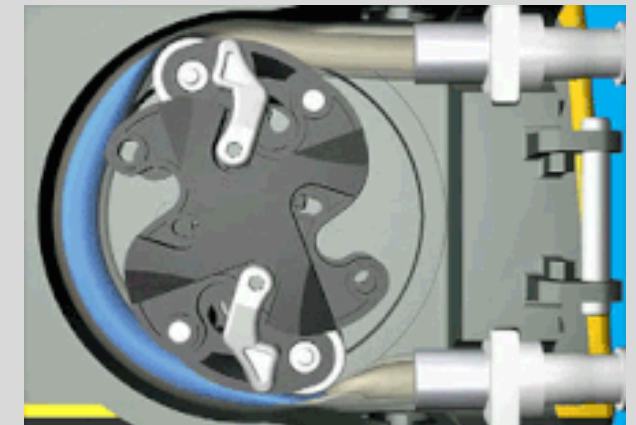
$$Q = 400 \frac{ml}{min} = 6.66 * 10^{-6} \frac{m^3}{s}$$

$$g = 9.81 \frac{m}{s^2}$$

$$p = 200 \text{mmHg} = 27 \text{kPa}$$

Assumptions:

- Velocity is same at inlet and exit
- No major or minor losses in pipe flow





# Engineering Calculations: Calcified Lesions

Part specifications for material hardness:

- High-hardness 3D printer filament
  - Shore 90A  $\approx$  Shore 39D [1]
- Fired Ceramic
  - Mohs 4  $\approx$  Shore 44D [2]
- Machined Steel (1045)
  - HB 215  $\approx$  Shore 33D [3]
- Target
  - HV 274  $\approx$  Shore 39D [9]

Conversions provided by

- [plantech.com](http://plantech.com)
- [www.efunda.com](http://www.efunda.com)
- [www.carbidepot.com](http://www.carbidepot.com)

# Engineering Calculations: Calcified Lesions

Minimum adhesion strength due to blood flow:

$$P_{min} = F/A$$

$$F = (1/2)Q\rho v \quad [4]$$

$$A = (1/2)\pi dL$$

$$Q = 8.183 \times 10^{-6} \text{ m}^3/\text{s} \quad [5]$$

$$\rho = 1060 \text{ kg/m}^3 \quad [6]$$

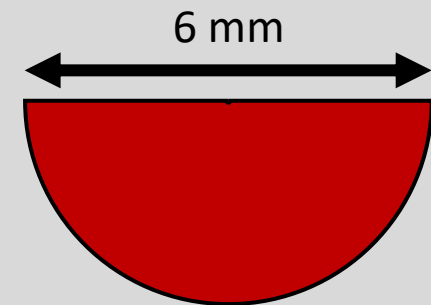
$$v = 0.2894 \text{ m/s}$$

$$d = 0.006 \text{ m} \quad [7]$$

$$L = 0.050 \text{ m}$$

- Assume maximum volumetric flow rate for blood
- Assume 50% occlusion, 6 mm diameter, and 5 mm length for calcified lesion

$$P_{min} = 26.63 \text{ Pa}$$



Femoral Artery Cross-Section

# Engineering Calculations: Blood Vessel

## Yield Strength

*The stress level where the blood vessel wall begins to deform plastically (no return).*

### -Mechanical Properties – Femoral Artery [22]

$d = 7$  to  $8$  mm (outer diameter)

$r = 3.5$  to  $4$  mm (radius)

$p = 200$  mmHg (femoral arterial diseased)

$t = 1$  mm (wall thickness)

Yield strength of filament:  $0.8$ MPa

We will design our vessel to not exceed the hoop stress value of  $93.45$ kPa for this will ensure no plastic deformation of the vessel.

## • Hoop Stress (Circumferential) [23]

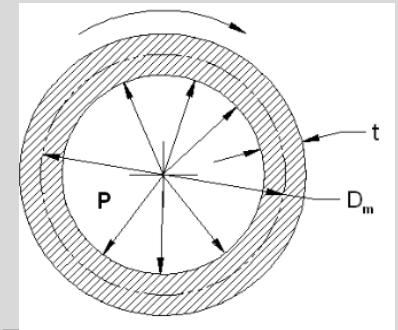
$p$  = internal pressure

$t$  = wall thickness

$r$  = inside radius

$D_m$  = mean diameter

$\sigma$  = hoop stress



$$D_m = \text{O.d.} - t = 8\text{mm} - 1\text{mm} = 7\text{mm}$$

$$\sigma = p * D_m / (2 * t)$$

$$\sigma = [(26.7\text{kPa}) * (0.007\text{m})] / (2 * 0.001\text{m})$$

$$\sigma = 93,450 \text{ Pa or } 93.45\text{kPa}$$

$$(\sigma)_{\text{axial}} = 46,725 \text{ Pa or } 46.73 \text{ kPa}$$

# Engineering Calculation: Filament

**Volume:**

$$\text{Solid Volume} = \frac{d^2 \pi L}{4} = \frac{8^2 * \pi * 12.4}{4} = 623.29 \text{ mm}^3$$

$$\text{Interior Volume} = \frac{d^2 \pi L}{4} = \frac{6^2 * \pi * 12.4}{4} = 350.601 \text{ mm}^3$$

$$\text{Volume of Hollow model} = \text{Solid Volume} - \text{Inner Volume} = 623.29 - 350.601 = 272.69 \text{ mm}^3$$

**Filament Required:**

$$\text{Volume} = \text{Filament Length} * \left( \frac{\text{Filament Diameter}}{2} \right)^2 * \pi$$

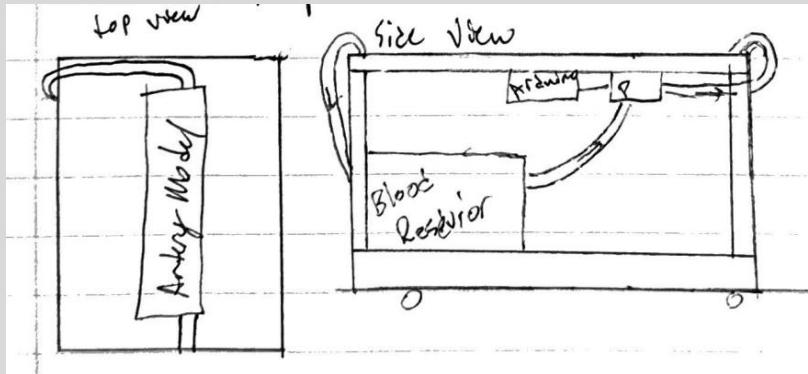
$$272.69 \text{ mm}^3 = \text{Filament Length} * \left( \frac{1.75}{2} \right)^2 * \pi$$

$$\text{Filament Length} = 113.37 \text{ mm or } 0.11337 \text{ m}$$

# Concept Evaluation: Top Level Design and Pump

## Top level design:

### Computing and pump undermounted

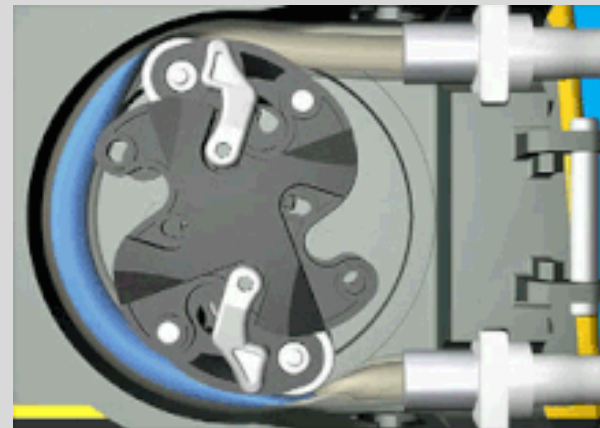


- Keeps computing unit and electronics out of the areas where fluid would rest if failure occurs
- Pump placement will be dependent on pump specs, calculations, and testing

## Pump selection:

### Peristaltic pump

- Pumps fluid without it contacting any machinery
- Precise flow rate is achievable through correct motor control



To start prototyping, a pump capable of 400ml/min flow rate will be purchased. After a proof-of-concept alternate pumps might be selected to better match blood flow properties

# Concept Evaluation: Calcified Lesions

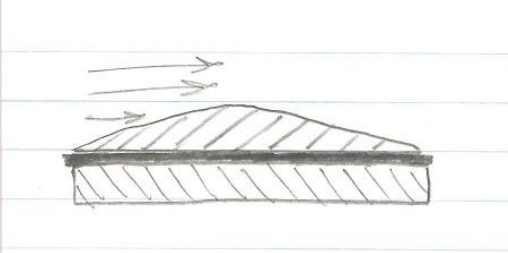
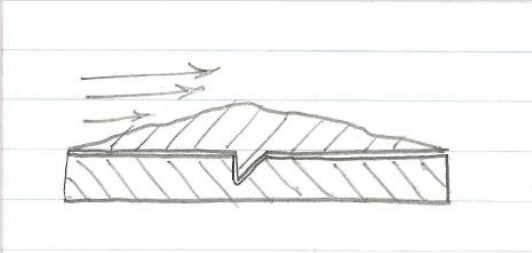
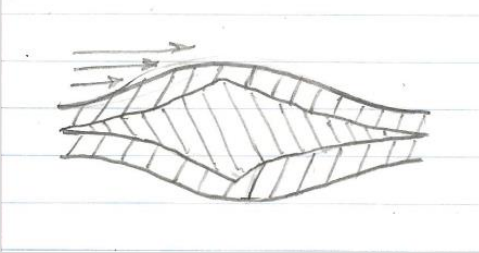
	High-Hardness 3D Printer Filament [1]	Fired Ceramic [2]	High-Hardness Machined Steel [3]
<b>Material</b>			
<b>Target</b>			
<b>Hardness: Shore 39D [9]</b>	Shore 39D	Shore 44D	Shore 33D
<b>Resolution: ~0.01 mm</b>	0.1 mm [10]	~1 mm	0.01 mm [11]
<b>Cost: &lt;\$1</b>	\$40/kg + manufacturing	\$7/kg + manufacturing	\$14/kg + manufacturing

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# Concept Evaluation: Calcified Lesions

- Modeling arterial calcified lesions is a novel feature not found in benchmarked designs. According to customer requirements, filament and ceramic best model simulated use conditions, filament and steel are the most replicable, and steel is the most durable.
- According to engineering requirements, filament most accurately and consistently models lesion hardness, filament and steel offer the highest resolution, and ceramic carries the lowest cost.
- Filament was chosen as lesion material due to its replicability, accurate modeling of simulated use conditions, high resolution, and desirable lesion properties, which were among the highest-weighted customer and engineering requirements.

# Concept Evaluation: Calcified Lesions




	Adhesive Paste	Interlocking Mechanism	Embedded
<b>Adhesion Method</b>			
<b>Target</b>			
<b>Adhesion Strength: &gt;27 Pa</b>	>27 Pa	>27 Pa	[Yield strength of vessel wall]
<b>Dimensions: ~0 mm</b>	~0 mm	~1 mm [12]	~0 mm
<b>Cost: &lt;\$1</b>	\$0.40/mL	negligible	negligible



# Concept Evaluation: Calcified Lesions

- Modeling arterial calcified lesions is a novel feature not found in benchmarked designs. According to customer requirements, paste best models simulated use conditions, mechanism is the most replicable, and embedded is the most durable.
- According to engineering requirements, paste and mechanism most accurately and consistently model lesion adhesion strength, paste and embedded require no protruding geometries, and mechanism and embedded require negligible additional cost.
- Paste was chosen as adhesion method due to its accurate modeling of simulated use conditions, lack of protruding geometries, and desirable adhesion strength, which were among the highest-weighted customer and engineering requirements.

# Concept Evaluation: Blood Vessel Structure

Material	Vinyl Tubing (PVC)	3D Printing Filament	Silicone Tubing
			
Customer Needs	Yes & No	Yes	Yes & No
Transparency	Exceptional	Exceptional	Translucent
Long Life Span	Exceptional	Exceptional	Exceptional

# Concept Evaluation: Blood Vessel Structure

## Specifications [25] :

- PETG Filament; produces a clear product
- Diameter = 1.75 mm (common)
- \$24.99/kg
- Hydrophobic (moisture-resistant)
- Strong adhesion factors
- Print temperature = 230 – 260 deg. C
- Tensile at yield = 0.8 MPa [24]

## Comparison:

- More control of vessel dimensions
- Less waste involved
- Better adhesion factors for lesion

## Hatchbox Transparent Filament



# Concept Evaluation: Blood Vessel Structure

Vessel Design Structure	Femoral Artery (R)	Lower Extremity	Femoral Artery
Customer Needs	Yes	No	Yes & No
Time Constraint	No	Yes	Yes & No
Material Constraint	No	Yes	No
Budget Constraint	No	Yes	No

# Concept Evaluation: Blood Vessel Structure

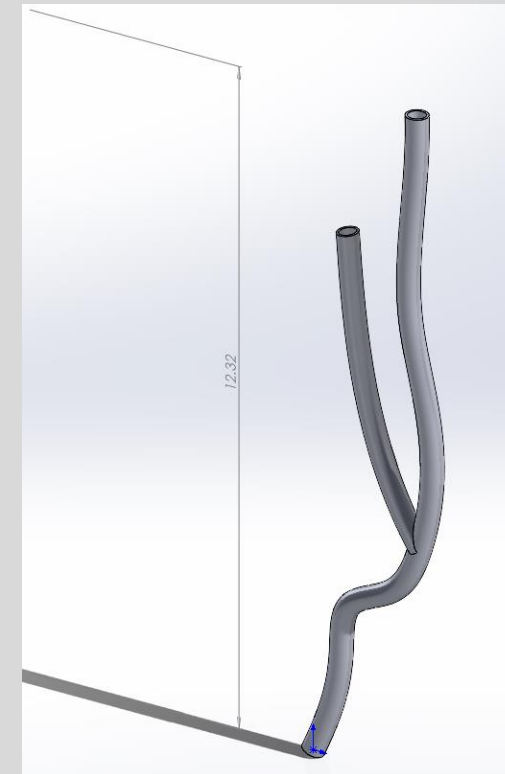
## Specifications (CAD):

- Density = 0.04 lbs/in<sup>3</sup>
- Mass = 0.03 lbs
- Volume = 0.74 in<sup>3</sup>
- Surface Area = 37.74 in<sup>2</sup>

## Comparison:

- Best at meeting customer needs
- Most cost effective
- Least at generating waste
- Best at avoiding constraints

## Femoral Artery (Right)



# Concept Evaluation: Blood Solution

## Material:

Glycerin



Simulated Blood



Corn Syrup, Water, Flour Mix



## Specification Requirements:

Density	1.26 g/mL	1.043-1.060 g/mL	Corn syrup- 1.37 g/mL (adjusted with water)
Cost	\$60	\$33	\$10
Viscosity	934 cP	N/A but states similar	Made to ideal
Solubility	High	Soluable	Good
Transparency	Yes	No	Yes mostly
Manufacturing	Pre-made	Pre-made	Mix ourselves

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# Concept Evaluation: Blood Solution

## Glycerin: Final Design Blood Analog



Density: 1.26 g/mL

Cost: \$60

Viscosity: 934 cP

### Final Design:

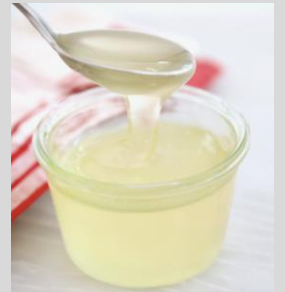
- Quantity with limited error in manufacturing
- Procedure for testing
- Much closer to blood specifications
- Available in desired quantity for reasonable price

## Corn syrup Solution: Prototyping Blood Analog

Density: 1.37 g/mL

Cost: \$10

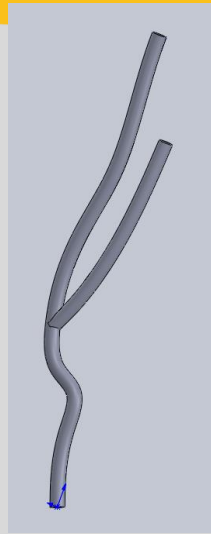
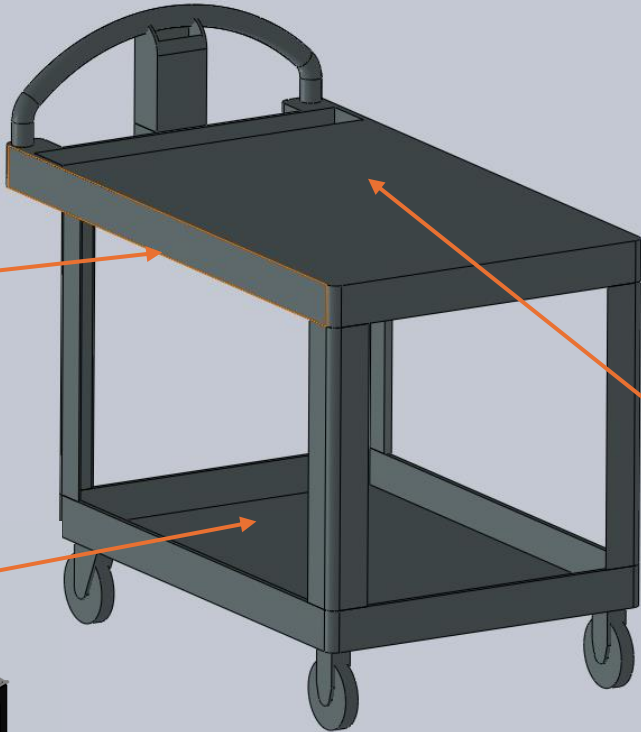
Viscosity: Similar but depends on the solution made



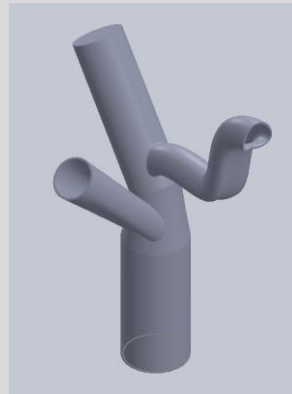
### Prototyping:

- Cost effective
- Simple to make
- Extreme case of blood thickness
- Limited mess/procedure for use

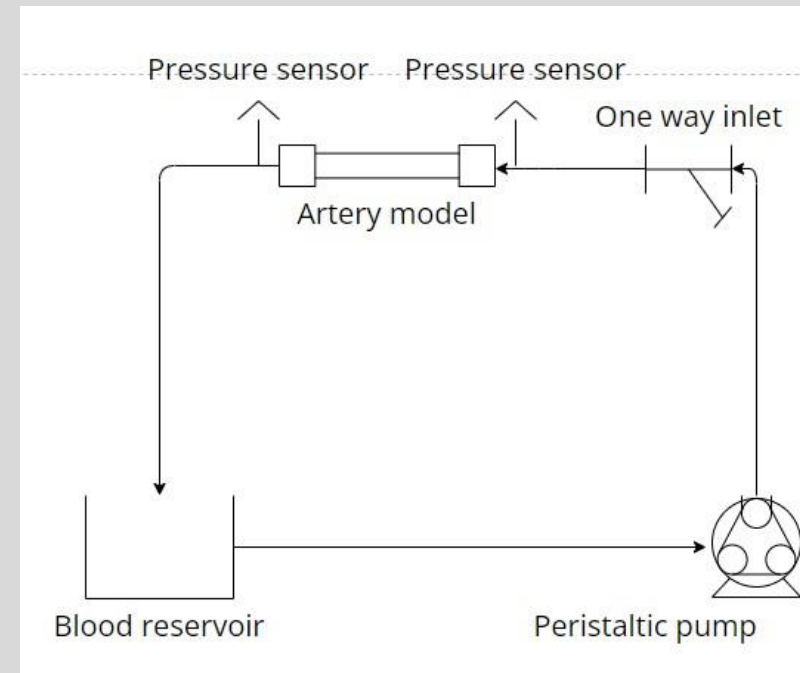
# Current State of Design



Vessels Systems



Pipe Flow Diagram:





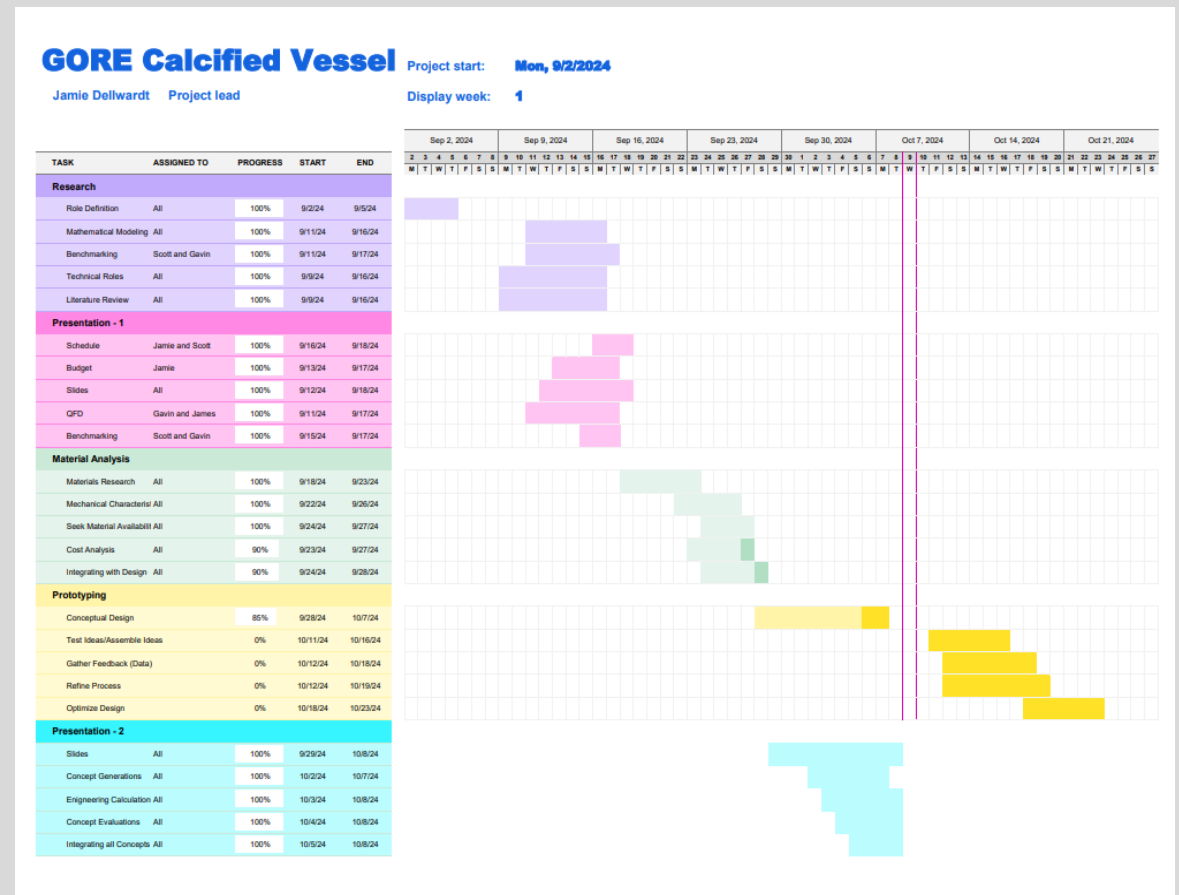
# Schedule – Gantt Chart

## Forecast:

- Prototyping phase
- Report 1

## Currently:

- ON schedule
- Need to begin prototyping
- Sub-concepts together to gear production towards final design



# BOM and Budget

## Bill of Materials

Item	Quantity	Cost Per Unit	Total Cost	% of Unit Cost
Pump	1	\$26.04	\$28.43	6%
Variable Power Supply	1	\$49.49	\$54.03	12%
85A Filament	1	\$51.43	\$56.15	12%
SainSmart TPU	2	\$24.63	\$53.78	12%
Tubing	2	\$6.99	\$15.26	3%
Cart/Platform	1	\$71.00	\$77.52	17%
Tank	1	\$42.49	\$46.39	10%
Sensing Unit	1	\$29.59	\$32.31	7%
Lesson Adhesive	1	\$9.50	\$10.37	2%
One way Inlet	1	\$9.03	\$9.86	2%
Artery Stand	1	\$15.00	\$16.38	4%
Blood Analog	1	\$33.25	\$36.30	8%
Syringes	100	\$14.99	\$16.37	4%
<b>Total Cost</b>			<b>\$453.15</b>	

## Budget

GORE Calcified		Income		\$3,000
Item	Quantity	Cost Per Unit	Total Cost	Notes
85A TPU Filament	1	\$51.43	\$56.15	Purchased
Peristaltic Pump	1	\$26.04	\$28.43	Purchased
Variable Power Supply	1	\$49.49	\$54.03	Purchased
SainSmart TPU	2	\$24.63	\$53.78	Purchased
Pump tank	1	\$26.24	\$28.65	
Syringes (100 count)	1	\$14.99	\$16.37	
Utility Cart	1	\$71.00	\$77.52	
Plastic tubing (12 m)	2	\$6.99	\$15.26	
Sensing Unit	1	\$29.59	\$32.31	
Lesson Adhesive	1	\$9.50	\$10.37	
One way Inlet	1	\$9.03	\$9.86	
Artery Stand	1	\$15.00	\$16.38	
Blood Analog	1	\$33.25	\$36.30	
Spent			\$192.40	
Total Predicted			\$435.41	
<b>Total Budget Remaining</b>			<b>\$2,564.59</b>	

# Thank You!

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